

Binding proteins internalized by PTD-fused ligands allow the intracellular sequestration of selected targets by ligand exchange

MARKUS A. MOOSMEIER^{1,2}, JULIA BULKESCHER¹, KARIN HOPPE-SEYLER¹ and FELIX HOPPE-SEYLER¹

¹Molecular Therapy of Virus-Associated Cancers (F065), German Cancer Research Center, Im Neuenheimer Feld 242, D-69120 Heidelberg, Germany

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Abstract. The targeted inactivation of intracellular molecules has important therapeutic potential. For this purpose, it could be envisioned to introduce specifically designed binding proteins into cells by covalent linkage to protein transduction domains (PTDs). However, stable linkage of a PTD to a cargo may affect its conformation and, hence, its binding property inside the cell. Here, we analyzed the ability of non-covalently linked PTDs to internalize the model binding proteins streptavidin (SA) and *Strep*-Tactin (ST). Notably, inside the cell, the PTD-*Strep*-tag II ligand used for internalization of SA was displaced by the model target biotin which exhibits a higher binding affinity for the same binding pocket. Thus, specifically designed binding proteins can be internalized into cells by non-covalent binding to a PTD and subsequently be used for capturing given intracellular target molecules by ligand exchange. Under therapeutic aspects, it could be envisioned to further develop such systems for the intracellular sequestration, and consequently, functional inactivation of pathologically relevant factors.

Introduction

Many therapeutic agents prescribed today belong to the group of cell-permeable small molecules which are derived from organics and peptides. In general, small molecules can enter the cell by simple diffusion and interact with intracellular targets in defined ways, for instance by blocking the target's active site with sufficient affinity or by irreversible covalent binding. However, many small molecules suffer from lack of specificity, leading to unwanted side effects and toxicity.

Macromolecular therapeutic agents based on proteins have several hypothetical advantages over small molecules

(1). Firstly, they possess a highly specific and complex set of functions that cannot be mimicked by small molecules. Secondly, since proteins target molecules in a highly specific way, they often have less potential to induce unspecific side effects than small molecules which can bind to similarly shaped pockets of proteins other than the target. Thirdly, protein therapeutics can provide effective replacement treatment for diseases in which proteins are mutated, truncated, or not expressed. On the other hand, however, most of the macromolecular therapeutic agents [e.g., antibodies (2), their fragments (3), or other proteins with specific binding potential (4), such as anticlins (5)] cannot penetrate cellular membranes of intact cells due to their biophysical properties (e.g., size, charge, and polarity). This restricts their use to extracellular proteins or to ectodomains of cell-surface receptors. Nevertheless, due to their potential advantages over small molecules, there has been growing interest in the use of therapeutic macromolecular agents against intracellular targets.

One way to induce cell membrane permeability of proteins is their covalent fusion to protein transduction domains (PTDs). PTDs are short peptides which enable internalization of linked molecules into a variety of eukaryotic cell types. An example of a well-studied cationic PTD is the Tat13 peptide (YGRKKRRQRRPP) which is derived from the HIV-1 *trans*-activator protein (6-10). Since the discovery of PTDs in 1988 (6,7), a broad range of bioactive proteins has been delivered into cells by this method, both *in vitro* and *in vivo* (11). This technology is thus considered to bear enormous potential to introduce macromolecular therapeutics into cells (12-14). Notably, PTDs may also penetrate intact epidermis and dermis which could enable transdermal delivery of cargos upon topical application (15-17).

However, the genetic fusion of PTDs to proteins can result in reduced protein expression and purification levels (10). Moreover, the stable linkage of PTDs, either by genetic or chemical means, can impair the biophysical properties of the cargo (10). Therefore, attempts have been made to generate universal cell permeable transporters that allow the concomitant internalization of cargos by non-covalent binding. Streptavidin (SA), an extracellular homotetrameric protein secreted by the bacterium *Streptomyces avidinii* (18), or SA fusion proteins were delivered into cells by PTD-biotin (19,20), on the basis of the high affinity of the SA/biotin

Correspondence to: Dr Markus A. Moosmeier, ²Present address: MorphoSys AG, Lena-Christ-Str. 48, D-82152 Martinsried/Planegg, Germany
E-mail: markus.moosmeier@morphosys.com

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interaction (21,22). The same SA binding pocket targeted by biotin is also reversibly bound by designed peptide motifs, such as *Strep*-tag II (WSHPQFEK) (23). In addition, *Strep*-tag II exhibits intrinsic affinity towards *Strep*-Tactin (ST), a derivative of SA (24). This *Strep*-tag II/ST system has become very common for one-step purification of proteins or high-affinity detection (23).

Here, we aimed to develop a novel two-component delivery system for the internalization of non-modified binding molecules (Fig. 1). The model system consists of the non-cell permeable SA protein containing a binding pocket for *Strep*-tag II which, in turn, is fused to a PTD. The same SA pocket is also bound by intracellular biotin, but with higher affinity. We hypothesized that, firstly, the PTD-*Strep*-tag II ligand should allow the cellular internalization of SA. Secondly, inside the cell, the PTD-*Strep*-tag II ligand should then be displaced by biotin. In principle, such systems could allow the sequestration and, consequently, functional inactivation of specific intracellular target molecules.

Materials and methods

Construction, expression, and purification of SA, ST, and Tat13-SA. The pET-21a plasmid (Novagen, Darmstadt, Germany) encoding core SA was kindly provided by P.S. Stayton. ST was expressed from the same vector backbone after QuikChange mutagenesis (Stratagene, Heidelberg, Germany) of the SA portion with primers 5'-G ACC GGT ACC TAC **ATC GGT GCG AGG GGT AAC GCT GAA TC**-3' and 5'-GA TTC AGC GTT ACC **CCT CGC ACC GAT GTA GGT ACC GGT C**-3' [bold letters indicate mutations to induce amino acid substitutions E⁴⁴I, S⁴⁵G, and V⁴⁷R which convert SA into ST (24)]. Tat13-SA was generated by PCR-amplification using *Taq* DNA polymerase (Invitrogen, Karlsruhe, Germany), the forward primer 5'-G GAA TTC CAT ATG TAC **GGA AGA AAG AAG CGC AGA CAA AGA AGA CGT CCA CCA GGT GCT GAA GCT GGT ATC ACC GGC ACC**-3' (bold letters denote the respective Tat13 PTD sequence), and reverse primer 5'-CGC AAG CTT TTA TTA GGA AGC AGC GG-3'. PCR-products were digested with *Nde*I and *Hind*III (New England Biolabs, Frankfurt, Germany) and subsequently ligated into linearized pET-21a. Correct sequences of the inserts were confirmed by DNA sequencing.

SA, ST, and Tat13-SA proteins were expressed in BL21(DE3) (Stratagene) as cytoplasmic insoluble inclusion bodies that were harvested, solubilised, refolded, and purified by fractionated ammonium sulfate precipitation (25). Proteins were finally dissolved in PBS buffer and stored at -80°C. Purified proteins were analyzed by sodium dodecyl sulfate polyacrylamide gel electrophoresis (SDS-PAGE), matrix-assisted laser desorption/ionization time of flight mass spectrometry (MALDI-TOF MS), Edman-sequencing, and circular dichroism (CD) spectroscopy (data not shown).

Peptide syntheses. Tat13-PEO₃-biotin and Tat13-*Strep*-tag II peptides were chemically synthesized at the Peptide Synthesis Core Facility of the German Cancer Research Center (Heidelberg, Germany) using Fmoc (N-(9-fluorenyl)methoxycarbonyl) chemistry. Crude peptides were purified by C₁₈ reversed phase

high-performance liquid chromatography (RP-HPLC) and analyzed by MS. Peptide stocks in DMSO (Merck, Darmstadt, Germany) were stored at -80°C and freshly diluted in H₂O.

Cell culture and transduction. HeLa cells were cultured in Dulbecco's minimal essential medium (DMEM, Gibco, Eggenstein, Germany), supplemented with 10% fetal bovine serum (FBS, PAA Laboratories, Pasching, Austria), 1% penicillin streptomycin sulfate, and 1% of 200 mM L-glutamine (Sigma-Aldrich, Taufkirchen, Germany), at 37°C in 5% carbon dioxide (CO₂) atmosphere. SA, ST, SA-horseradish peroxidase (HRP, Pierce, Rockford, IL, USA), or ST-HRP (IBA, Göttingen, Germany) proteins were complexed with biotin (Supelco, Bellefonte, PA, USA), *Strep*-tag II (IBA), Tat13-PEO₃-biotin, or Tat13-*Strep*-tag II by incubation for 15 min at room temperature. The complexes were directly injected into FBS-free DMEM medium.

Thermal tetramer stability. Purified SA/ST proteins (3 µg) without or with a 2-fold molar excess of biotin, or *Strep*-tag II, were combined with SDS-containing sample buffer and heated at selected temperatures for 5 min, then chilled on ice, and subsequently analyzed by SDS-PAGE. Proteins were stained with Coomassie brilliant blue (Serva, Heidelberg, Germany).

Western blotting. Protein extracts (2 µg) were combined with SDS-containing sample buffer and boiled at 85 and 99°C for 5 min, separated by 15% SDS-PAGE, transferred in a semi-dry blotter system (cti, Idstein, Germany) to an Immobilon-P membrane (Millipore, Billerica, MA, USA), and analyzed by enhanced chemiluminescence (GE Healthcare, Munich, Germany). The following antibodies were used: rabbit anti-SA antibody (Sigma-Aldrich, 1:2000), mouse anti-tubulin antibody CP06 (Calbiochem, Schwalbach, Germany, 1:5000), and anti-mouse and anti-rabbit HRP-labeled secondary antibodies (Promega, Mannheim, Germany, 1:3000).

Fluorescence microscopy. HeLa cells were plated on 35 mm dishes (Greiner Bio-one, Frickenhausen, Germany) at 40-60% confluency. SA/ST proteins (10 µM) were complexed with 10 µM Tat13-PEO₃-biotin or Tat13-*Strep*-tag II and directly injected into FBS-free media. After a 120-min incubation at 37°C, 5% CO₂, the cells were washed, trypsinized, plated on glass cover-slips, and fixed with 4% paraformaldehyde (Merck, Darmstadt, Germany) after 4 h. Cover-slips were stored at -20°C in 70% ethanol. Internalized SA and ST proteins were detected using a rabbit anti-SA antibody (1:500) and an anti-rabbit Cy3-labeled secondary antibody (Dianova, Hamburg, Germany, 1:400). Cy3-signals were detected using a Vanox-T fluorescence microscope (Olympus, Hamburg, Germany) and an F-View camera (Olympus).

HRP assay. HeLa cells were plated on 35 mm dishes at 80-90% confluency and treated with 1 µM SA-HRP or ST-HRP complexed with 2 µM Tat13-PEO₃-biotin or Tat13-*Strep*-tag II. Cells were incubated at 37°C, 5% CO₂ for 2 h, then trypsinized, washed with 1X PBS, and lysed with 400 µl 1X reporter lysis buffer (RLB, Promega). Cell lysates were incubated at room temperature for 15 min. After vortexing and pelleting, the supernatants were stored at -80°C. Extracts were diluted and

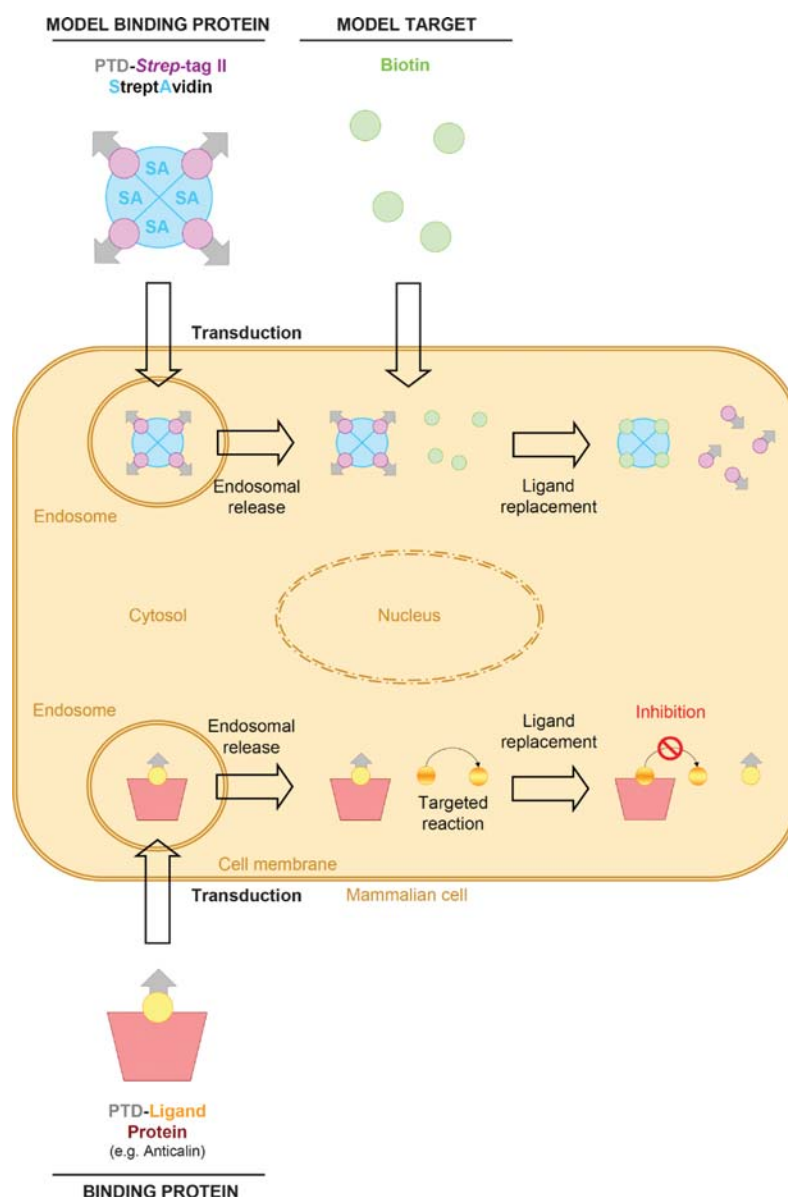


Figure 1. Model for the internalization of SA by PTD-fused *Strep-tag II* (upper part of the panel). SA is internalized into mammalian cells most likely via the endosomal route. In the cytoplasm, PTD-*Strep-tag II* is replaced by the higher affinity ligand biotin whose internalization is supported by means of the multivitamin transporter. If this system is principally functional, one could envision the application of therapeutically useful binding molecules, e.g., anticalins, using low affinity PTD-ligands for internalization (lower part of the panel). Subsequently, this ligand will be replaced by a higher affinity intracellular target molecule, leading to the functional inactivation of the latter by sequestration.

40 μ l thereof were mixed with 10 μ l 1X RLB. At the same time, and under identical conditions, calibration curves were generated using a series of dilutions of SA-HRP or ST-HRP. SA-HRP and ST-HRP fusion proteins were diluted and 10 μ l thereof were supplemented with 40 μ l of dilutions of untreated HeLa lysates. Colorimetric reactions were initiated by adding 50 μ l of 1-Step Ultra TMB-ELISA substrate solution (Pierce). The reaction was stopped by adding 50 μ l of 2 M sulfuric acid (Merck) and the absorbance was measured at 450 nm. Calibration curves were fitted using the four parameter logistic (4PL) equation in SigmaPlot 10.0 (Systat Software, Erkrath, Germany). The absorbance was recalculated to the amount of internalized HRP and normalized to the amount of total protein determined by Bradford protein assay as described (26).

Results

Intracellular distribution of SA and ST internalized by Tat13-fused ligands. To investigate the uptake and intracellular distribution of model proteins by non-covalent PTD linkage, we analyzed SA and the SA-derivate ST, upon non-covalent linkage to different ligands fused to the Tat13 PTD.

HeLa cells were incubated with 10 μ M SA pre-complexed with 10 μ M Tat13-PEO₃-biotin. Non-complexed SA served as negative control. After 2 h of incubation, cells were trypsinized to remove extracellularly attached proteins, plated on glass coverslips for fixation, and subsequently analyzed by immunofluorescence. It was found that Tat13-PEO₃-biotin internalized its cargo SA into virtually 100% of the HeLa cells (Fig. 2A).

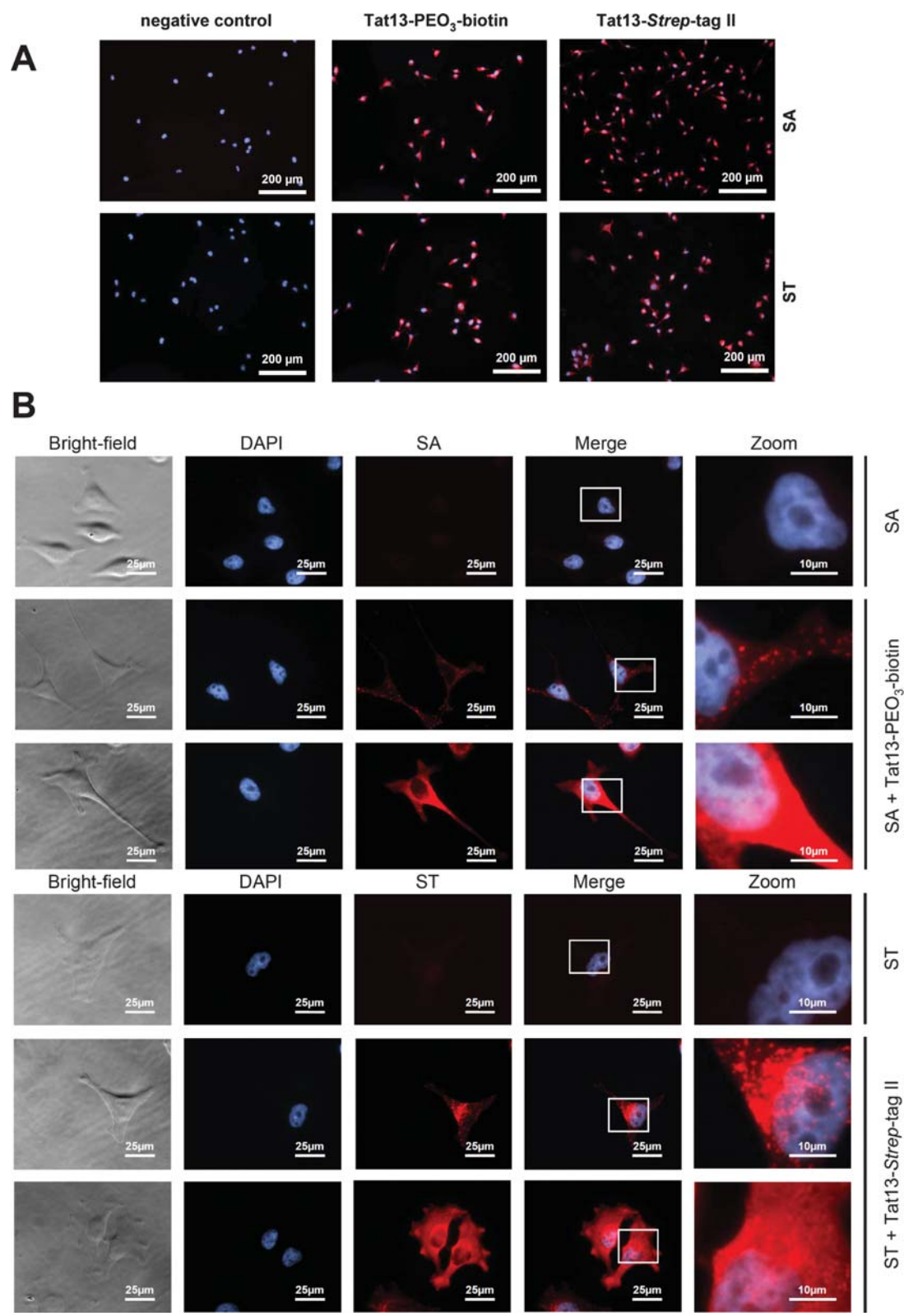


Figure 2. Immunofluorescence studies analyzing SA and ST internalization. (A) Uptake of SA or ST mediated by the Tat13-fused ligands biotin or *Strep*-tag II. Negative control, treatment of the cells with SA and ST in the absence of PTD-fused ligands. SA and ST were detected using an anti-SA antibody, DNA was stained with DAPI. (B) Larger magnifications to assess the intracellular distribution. SA and ST proteins internalized by PTD-fused ligands exhibited either a punctuated pattern around the cell nucleus or diffuse cytosolic staining. Zoom, higher resolution of boxed areas.

In contrast, control cells treated with SA in the absence of Tat13-PEO₃-biotin showed no internalization. Higher resolution microscopy analyses showed that Tat13-internalized SA was typically detected in two major intracellular distribution

patterns (Fig. 2B), either punctuated around the cell nucleus and/or solubilized in the cytosol. These patterns are typical for PTD-internalized cargos, reflecting their entrance via the endosomal route (27).

Table I. Quantification of the internalization of SA and ST by Tat13-fused ligands.

HRP-fused	Tat13-fused	K _D (μ M)	Quantification (pmol/mg)
SA	PEO ₃ -biotin	10 ⁻⁸	26-72
ST	PEO ₃ -biotin	<1	22-29
ST	<i>Strep</i> -tag II	1	4.2-14
SA	<i>Strep</i> -tag II	72	0.56-1.5

Internalized amounts of HRP were calculated in pmol of internalized SA-HRP or ST-HRP, normalized to the total amount of protein.

Notably, ST could also be efficiently internalized into cells by non-covalent binding to its ligand *Strep*-tag II, fused to the Tat13 PTD (Fig. 2A). This is remarkable, since the binding affinity between ST and *Strep*-tag II ($K_D = 1 \mu\text{M}$) (23) is substantially lower than the affinity between SA and biotin ($K_D = 10^{-14} \text{ M}$) (17). HeLa cells treated with complexes of ST and Tat13-*Strep*-tag II were almost 100% ST-positive (Fig. 2A) and exhibited the same intracellular distribution as observed for SA introduced by Tat13-PEO₃-biotin (Fig. 2B).

Finally, the internalization of SA by Tat13-*Strep*-tag II [$K_D = 72 \mu\text{M}$ (28)] and ST by Tat13-PEO₃-biotin ($K_D < 1 \mu\text{M}$) was tested. Again, HeLa cells were almost 100% positive for the SA or ST cargos, respectively, after treatment with the

corresponding complexes (Fig. 2A). Control-treated cells showed no cargo internalization (Fig. 2A). Taken together, these results demonstrate efficient internalization of both SA and ST by non-covalently bound PTDs.

Quantification of internalization. To estimate the efficiency of transmembrane delivery, horseradish peroxidase (HRP) fused to SA or ST was applied as cargo. HeLa cells were incubated with $1 \mu\text{M}$ of SA-HRP or ST-HRP complexed with $2 \mu\text{M}$ Tat13-fused ligands. Substantial enzymatic HRP activities were measured only in lysates of HeLa cells treated with SA-HRP or ST-HRP if complexed with the respective Tat13-ligands (data not shown). SA-HRP and ST-HRP calibration curves were calculated to estimate the amount of Tat13-mediated internalization. The internalization rates were quantified with respect to the amount of functional SA-HRP and ST-HRP in pmol, and normalized to the total amount of protein (Table I). The internalization efficiencies of ST-HRP by Tat13-*Strep*-tag II were lower than those of SA-HRP internalized by Tat13-PEO₃-biotin, in line with the different ligand affinities (see above).

Ligand replacement by an intracellular target. Next, we tested whether a binding protein internalized by non-covalent binding to a PTD-fused ligand could be utilized to sequester an intracellular target by ligand replacement. As model systems, we employed SA and ST internalized via their ligand *Strep*-tag II linked to the Tat13 PTD (schematic model in Fig. 1). We then tested whether Tat13-*Strep*-tag II was replaced by intracellular biotin which binds to the same pocket as *Strep*-tag II, but with higher affinity (22,23).

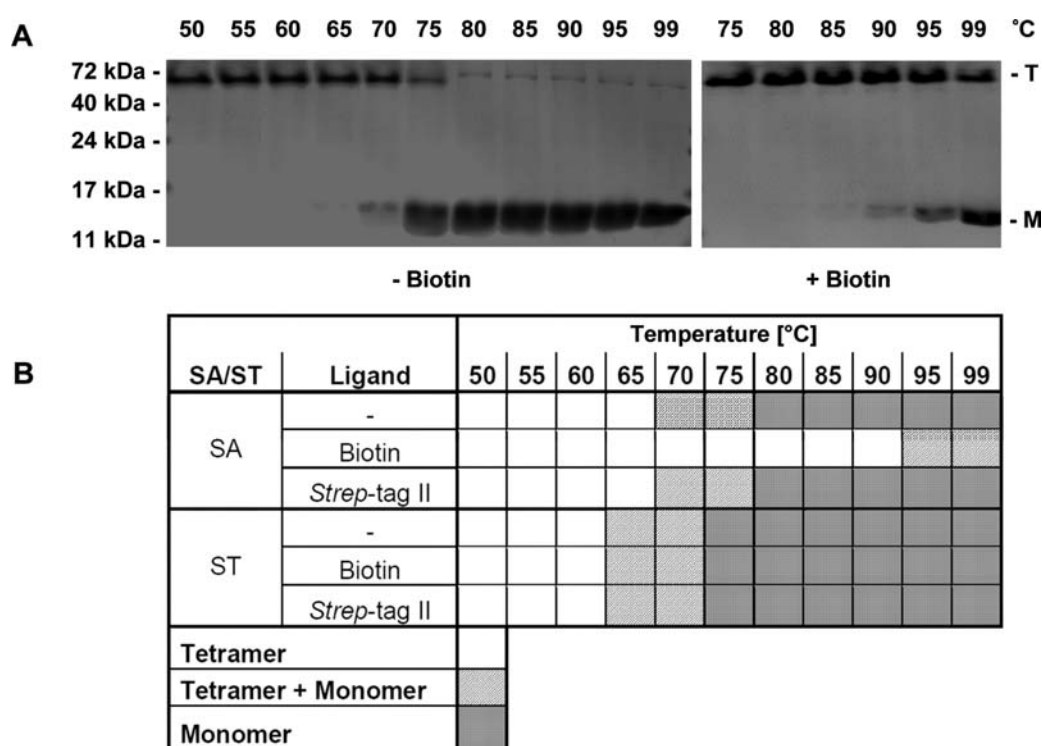


Figure 3. Thermal tetramer stability of SA and ST. (A) Exemplary SDS-PAGE analyses of Coomassie-stained SA in the absence of a ligand (left panel) or after addition of biotin (right panel). Tetrameric (T) and monomeric (M) states are indicated. (B) Compilation of thermal stabilities of SA and ST, either in the absence or presence of the ligands biotin and *Strep*-tag II.

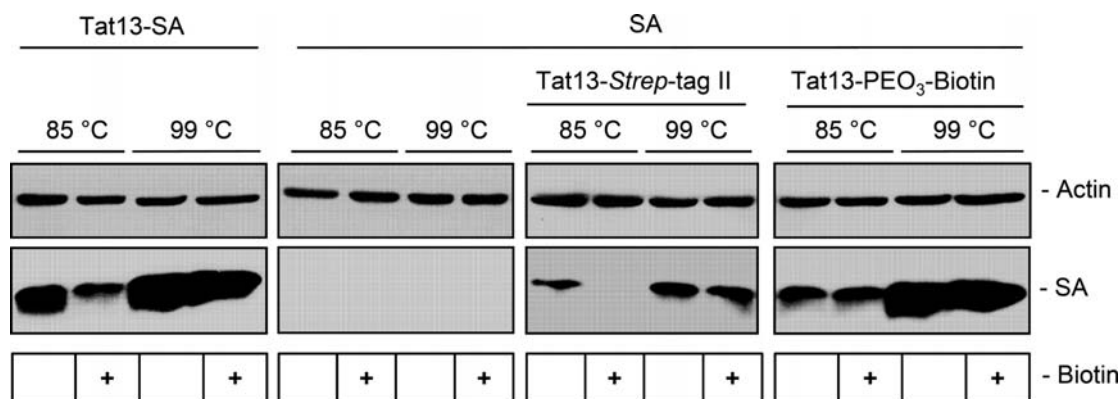


Figure 4. Intracellular replacement of Tat13-*Strep*-tag II on SA by biotin. Immunoblot analysis of monomeric SA. SA was internalized by covalently bound Tat13 or by non-covalently linked Tat13-*Strep*-tag II or Tat13-PEO₃-biotin. Actin, loading control.

First, it was necessary to investigate whether the ligand-linked PTDs might affect SA or ST tetramerization (24) which is required for building the binding pocket for biotin and *Strep*-tag II (29). SA and ST tetramers are extremely stable even in the presence of SDS and therefore can be detected on SDS-polyacrylamide gels (30,31). Temperature-dependence of tetramer breakup was studied by heating and subsequent SDS-PAGE analyses. Up to a temperature of 65°C, SA proteins were detectable solely in a tetrameric state (Fig. 3). The amino acid substitutions to convert SA into ST decreased the tetramer stability by 5°C (Fig. 3B). The pre-incubations of ST with biotin or *Strep*-tag II had no effect on the temperature-dependent ST tetramer breakup. Likewise, pre-incubation of SA with *Strep*-tag II peptides induced no changes in the temperature-dependent SA tetramer breakup. Notably, however, SA complexed with biotin showed an increased tetramer stability up to 90°C (Fig. 3), as previously reported (31). This increased tetramerization can be readily visualized by the strongly reduced amounts of monomeric SA at higher temperatures (Fig. 3A), thereby providing a readily accessible readout for the biotin/SA complex formation.

As a positive control for cellular assays (Fig. 4), HeLa cells were treated with 10 μ M Tat13-SA where the PTD is covalently linked to SA. After 2 h, cells were extensively washed and, subsequently, 40 mM biotin was added to the cells. Biotin-uptake was supported by means of the mammalian multivitamin transporter (32). After 2 additional hours, cell lysates were prepared and analyzed by immunoblotting. Addition of biotin to the cells resulted in a clear reduction of SA monomers at 85°C (Fig. 4), reflecting increased tetramer stability.

Next, HeLa cells were treated with complexes of 10 μ M SA and 20 μ M Tat13-*Strep*-tag II. As observed for the positive control, intracellular SA tetramers were thermally stabilized by the addition of biotin to the cells, as indicated by the decreased amount of SA monomers at 85°C (Fig. 4). These findings show that the same binding pocket which has been used for SA internalization by a non-covalently bound ligand can be used for intracellular sequestration of an higher affinity target.

As further control, we employed Tat13-PEO₃-biotin-internalized SA. Since Tat13-PEO₃-biotin, as a biotin-derivative, already strongly binds to the SA pocket, it would be expected

that addition of biotin to the cells does not further increase thermal stabilities. Indeed, and in contrast to Tat13-SA or SA introduced by Tat13-*Strep*-tag II, the Tat13-PEO₃-biotin-internalized SA was not thermally stabilized by the addition of biotin to the cells (Fig. 4).

Taken together, these results strongly suggest that intracellular biotin induced the thermal stabilization of SA tetramers by replacing Tat13-*Strep*-tag II on SA. Thus, the internalization of a binding protein by a low affinity ligand fused to a PTD is feasible and can be utilized for subsequent ligand replacement inside the cell (Fig. 1).

Discussion

The delivery of molecules into cells poses a major problem that has to be solved for the development of therapeutic agents acting on intracellular targets. Cargos which cannot penetrate cellular membranes by themselves due to their biophysical properties can achieve cell membrane permeability by fusion to PTDs (11). Notably, however, the design and generation of PTD-fused proteins can result in reduced expression and purification levels and/or in altered biophysical properties of cargos (10). Therefore, a transporter system for the transmembrane delivery of non-modified cargos was developed. It aimed at a PTD-mediated internalization of a non-covalently linked protein which can capture an intracellular target molecule by ligand exchange.

The components of this model system consisted of: i) SA, a model binding protein containing a binding pocket for its intracellular target biotin, ii) the PTD-fused ligand *Strep*-tag II, a cell-permeable transporter which more weakly interacts with the same pocket, and iii) biotin, which should replace the PTD-*Strep*-tag II ligand at the intracellular level due to its higher binding affinity to SA. Both immunoblot and immunofluorescence analyses demonstrated that Tat13-*Strep*-tag II mediated the successful transmembrane delivery of non-covalently bound SA. Moreover, supplemented biotin displaced the Tat13-*Strep*-tag II ligand as confirmed by an increased thermal tetramer stability of internalized SA.

The internalization of SA and ST by non-covalent linkage to Tat13-fused ligands was found to be highly efficient in that almost 100% of the treated cells were positive for SA

or ST. Similar efficiencies have been reported for the use of covalently linked PTDs (33). The internalization efficiency by Tat13-fused *Strep*-tag II was further quantified using functionally active HRP fused to SA. It was lower (~1 pmol per mg of total cellular protein) than the reported efficiency of the internalization of FITC-SA by Tat11-biotin (23 pmol/mg) (26). This could be explained by the >2-fold increased MW of SA-HRP (~134 kDa) above FITC-SA (~60 kDa) and by the law of mass action.

The system developed in the present work provides some important advantages over existing transporter systems. Firstly, it allows the delivery of a non-modified cargo and avoids potential problems associated with the covalent linkage of a PTD, such as reduced expression and purification yields and impairment of the biophysical properties of the cargo (10). Secondly, in contrast to previously designed transmembrane delivery systems, such as Tat11-SA for biotinylated molecules (27,34) or Tat11-fused protein A for antibodies (35,36), the transporter employed here is less bulky since it only consists of low-MW components: a PTD and a small ligand. Thirdly, since the active site of the internalized cargo is reversibly occupied by a PTD-fused ligand, only molecules possessing a higher affinity to the cargo should be able to displace the ligand which increases specificity.

Taken together, the findings of this study indicate that, in principle, various engineered binding molecules, such as anticalins (5,37) (Fig. 1) or peptide aptamers (38), could be tailored for the intracellular sequestration of a given target molecule by similar strategies. For example, specific binding proteins could be internalized by a PTD-fused ligand which is derived from a natural interaction partner of the binding protein, but exhibits reduced binding affinity due to chemical modifications. After PTD-mediated internalization, this weakly bound ligand should be displaced by the higher affinity intracellular target, as shown here for the replacement of PTD-*Strep*-tag II by biotin.

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