Pathologic analysis of glioblastoma via multiple stereotactic biopsies of active tumor and necrosis

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Received August 11, 2011; Accepted October 3, 2011

DOI: 10.3892/or.2011.1522

Abstract. To obtain more representative biopsy specimens in glioblastoma, we performed multiple stereotactic biopsies of active tumor and necrosis. We investigated their pathologic differences of diagnosis and also examined the pathologic features that varied with ¹¹C-methionine uptake on PET. From December 2009 to October 2010, we performed stereotactic biopsies in 12 patients with radiologically heterogeneous, ringenhanced lesions. We biopsied the MR enhanced lesions for active tumor and the MR non-enhanced lesions for necrosis and analyzed differences of pathologic diagnoses between them. As correlating factors of the degree of ¹¹C-methionine uptake (T/N ratio), the pathologic findings, including cell density, Ki-67 LI, microvessel density, number of endothelial proliferations, the immunopositivity for L-amino acid transporter 1 (LAT1) were analyzed. The final diagnosis of each specimen was glioblastoma. The diagnostic failure rate was 33.3% (4/12 patients) when we selected only active tumors and 40% (4/10 patients) when we selected necrotic lesions. The T/N ratio showed a statistical correlation with cell density depending on the degree of necrosis and LAT1 immunopositivity (P=0.002 and 0.032). LAT1 was localized in the tumor cells, vascular endothelium, and the vicinity of endothelial proliferation. Multiple stereotactic biopsies of active tumor and necrosis could provide the diagnostic yield in glioblastoma. The ¹¹C-methionine uptake mostly reflected cell densities depending on the degree of necrosis.

Introduction

Stereotactic brain biopsy is a minimally invasive form of diagnostic technique that uses a three-dimensional coordinate

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system to locate small targets inside the brain. Magnetic resonance imaging (MRI) provides sharp anatomical details of the pathologic brain and stereotactic operations generally use MRI. However, an inaccurate diagnosis or underestimation of a lesion's pathological grade sometimes occur because clinicians can get only a small amount of tissue to represent the lesion's total features (1-3). Even if the clinician has a provisional radiological diagnosis of high-grade glioma, the pathologist may confirm a low-grade glioma from the small specimen. Gliomas, especially, are histologically heterogeneous, and inadequate localization of the stereotactic biopsy may produce specimens that are irrelevant for identifying and grading the lesions (4). Endothelial proliferation and/or necrosis are essential diagnostic features for the pathological diagnosis of glioblastoma. On enhanced MR images, an enhanced lesion corresponds to a cellular, highly vascularized area of the neoplasm and a non-enhanced lesion corresponds to a necrotic or cystic lesion, with decreased vasculature (5). Therefore, to obtain more representative biopsy specimens, we biopsied the MR enhanced lesions for active tumor and the MR non-enhanced lesions for necrosis to cover the important pathologic features and investigated their pathologic differences of diagnosis.

¹¹C-methionine uptake is regulated by an amino acid transporter at the endothelium surface, and L-type amino acid transporter 1 (LAT1) is a major route for the transport of large neutral amino acids, including methionine (6,7). This uptake reflects the tumor cell density, proliferative potential and angiogenic capability of gliomas (8-11). We also examined the pathologic features that varied with ¹¹C-methionine uptake.

Materials and methods

Patients and stereotactic biopsy. From December 2009 to October 2010, we performed stereotactic biopsies in 12 patients who had radiologically high-grade gliomas at Chonnam National University Hwasun Hospital. To determine locations for the tumor biopsies, we employed contrast-enhanced T1-weighted images. ¹¹C-methionine PET was also performed. To obtain tissue with high diagnostic value, we aimed in each case for the active lesion, contrast-enhanced area on MRI; to obtain the necrotic lesion, we targeted a non-enhanced area

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Key words: biopsy, ¹¹C-methionine PET, enhanced MRI, glioblastoma, LAT1, stereotactic

(Fig. 1A and C). Three to four core biopsies were taken from each target. Two patients underwent biopsy of a single area because of bleeding. However, there was no significant bleeding due to increased intracranial pressure. A Leksell stereotactic apparatus guided the biopsy, under local anesthesia.

¹¹*C*-methionine positron emission tomography. The [¹¹C]CO₂ was produced by irradiating N₂ gas with 16.4 MeV protons accelerated in a cyclotron (General Electric, USA). [¹¹C]CO₂ was converted to [¹¹C]CH₄ using nickel, under hydrogen gas and subsequently converted to [¹¹C]CH₃I by reacting it with Iodogen. Finally, the [¹¹C]CH₃I was reacted on a solid phase extraction cartridge containing L-homocysteine thiolactone solution in ethanol, synthesizing [¹¹C]MET via the S-methylation of L-homocysteine in the presence of a potassium hydroxide base. After neutralization with 1 N HCl, the [¹¹C]MET was filtered through 0.22 μ m filters. Via the analytical HPLC system, we confirmed the prepared [¹¹C] MET's radiochemical purity was above 95%.

We performed the PET with a dedicated PET/CT scanner by GE Medical Systems (Discovery ST, GE Medical Systems, Milwaukee, WI, USA), with a spatial resolution of 5.0 mm (full width at half maximum) and slice thickness of 3.27 mm. Patients were placed in the scanner such that slices parallel to the orbitomeatal line could be obtained. We intravenously injected patients with ¹¹C-MET during a fasting period, at 7 MBq/kg. For attenuation correction, we acquired a non-contrast-enhanced, low-dose CT scan and then began the 10 min emission scan 20 min after the injection. We reconstructed the images in the form of transaxial images of 256x256x98 anisotropic voxels (the voxel size was 1.17 mm x 1.17 mm x 3.27 mm) with OSEM (ordered subset expectation maximization: iteration, 5; subset, 32) and used CT images for attenuation correction of the PET images.

Magnetic resonance imaging. All MR images were obtained using a 1.5-T (Signa Excite Twin Speed, GE Medical Systems, Milwaukee, WI, USA) whole-body MR scanner, with an acquisition time of ~3 min.

Image analysis. After obtaining the PET data, we registered the PET image on contrast-enhanced, T1-weighted standard anatomical MRI images, using normalized mutual information from the Leksell Gamma Plan 8.3.1 image registration software (Elekta Instrument AB, Stockholm, Sweden). We manually placed the regions of interest (ROIs) and the contralateral grey matter in the axial plane. The maximal standardized uptake value (SUVmax) was calculated over the ROI of each targeted lesion. The tumor-to-normal tissue (T/N) ratio was calculated by dividing the SUVmax of the lesion by the SUVmean of the contralateral gray matter.

Pathologic reviews and immunohistochemical staining. Tumor samples, obtained during surgery, were formalin-fixed and paraffin-embedded for the histological studies. Two independent neuropathologists re-evaluated each histological diagnosis and graded it according to the 2007 WHO classification (5). We compared the histopathologic examinations between radiologically different targets (Fig. 1B and D). The neuropathologists examined the pathologic specimens for atypism (positive/negative), mitosis (positive/negative), endothelial proliferation (positive/negative) and necrosis (positive/negative). We estimated the number of endothelial proliferations per mm² and the cell density, depending on the necrotic extent: (grade 1) cystic fluid, (grade 2) tumor cells with necrosis \geq 95%, (grade 3) tumor cells with 50% \leq necrosis <95%, (grade 4) tumor cells with 25% \leq necrosis <50%, (grade 5) tumor cells with necrosis <25% or (grade 6) tumor cells with focal necrosis.

For the immunohistochemical staining, we excluded specimens having over 50% necrosis and formalin-fixed and paraffin-embedded the remaining specimens, cutting them to a thickness of 5 μ m. In the deparaffinized sections, endogenous peroxidase was blocked with 3% H₂O₂ in methanol. We carried out the antigen retrieval for 30 min, in a pressure cooker with Tris buffer and blocked non-specific binding for 10 min, using protein-blocking buffer. Sections were washed in phosphatebuffered saline (PBS) and incubated overnight with anti-human L-type amino acid transporter 1 (LAT1) antibody (dilution: 1:400, clone 4D9, Trans Genic, Inc., Kobe, Japan), human Ki-67 antibody (dilution: 1:100, M7240, Dako) and Von Villebrand factor (dilution: 1:50, Clone F8/86, Dako), at 4°C. The samples were then incubated with a secondary antibody (biotinylated link) for 10 min, with streptavidin-HRP for 10 min, and then with diaminobenzidine (DAB), which was used as a chromogen. All chemicals were obtained from the LSAB system (DakoCytomation; Dako, Glostrup, Denmark). Counter-staining was performed with Mayer's hematoxylin (Fig. 2).

We semi-quantitatively evaluated LAT1's immunopositivity by estimating the fraction of positive cells, regarding a level <5% as negative expression (grade 1), a level <50%as a moderate degree of expression (grade 2) and a level of \geq 50% as a high degree of expression (grade 3). To measure each glioma's microvessel density (MVD), we used the method described by Zhen et al and Leon et al (12,13). Briefly, in areas of the most intense neovascularization, we performed individual microvessel counts at x200 magnification (equivalent to 0.7386 mm²). Any endothelial cell or endothelial cell cluster was considered as a single countable microvessel. MVD was expressed as the absolute number of microvessels per x200 field for each case. We also counted the Ki-67 labeled cells and calculated the percentage of Ki-67 labeled cells within the observed field, regarding a level <5% as grade 1, a >5% to <25% as grade 2, a >25% to <50% as grade 3, and a level of \geq 50% as grade 4.

Statistical analysis. Statistical analysis was performed with the SPSS software program (version 18.0 for Windows; SPSS, Inc., Chicago, IL, USA). We used multiple linear regression to analyze the enhancement, cell density, microvessel density, immunopositivity of LAT1, Ki-67 LI and the number of endothelial proliferations as the correlating factors of the T/N ratio. A P-value of <0.05 was considered statistically significant.

Results

Pathologic analysis corresponding to active or necrotic lesions. Pathologic analysis is summarized in Table I. Male to female ratio was 6:6 and median age was 65 years (range: 55-77 years). The final diagnosis of all specimens was

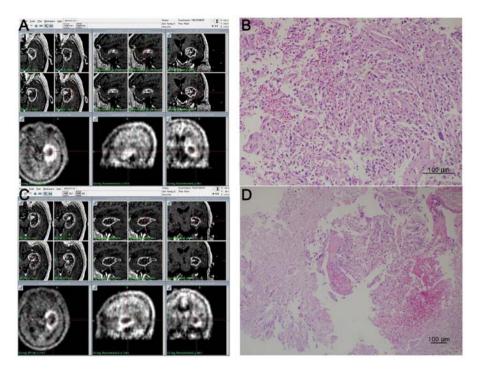


Figure 1. Radiologic targets (red cross) for biopsy with Leksell Gamma Plan images. (A) MR contrast-enhanced area for active tumor and ¹¹C-methionine-PET image (T/N ratio=2.91). (B) Pathologic review for target A: atypism (positive), mitosis (positive), endothelial proliferation (positive) and necrosis (positive). (C) MR non-enhanced area for necrosis and ¹¹C-methionine-PET image (T/N ratio=0.68). (D) Pathologic review for target C: atypism (negative), mitosis (negative), endothelial proliferation (positive) and necrosis (positive).

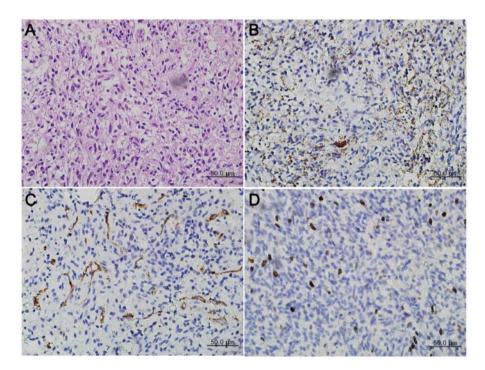


Figure 2. Immunohistochemical staining for L-type amino acid transporter 1 (LAT1), Von Villebrand factor and Ki-67 antigen. (A) Hematoxylin and eosin staining for glioblastoma. (B) Immunohistostaining for LAT1 (grade 2). (C) Immunohistochemical staining for Von Willebrand factor (81.2/mm²). (D) Ki-67 antigen (grade 2).

glioblastoma as below criteria (atypism/mitosis/endothelial proliferation/necrosis).

When we chose the MR-enhanced active lesions as targets, in a total of 12 patients, we diagnosed eight patients with glioblastoma, three with anaplastic astrocytoma and one with astrocytoma. When we chose only one enhanced lesion for biopsy, the glioblastoma diagnosis failure rate was 33.3%(4/12 patients). For the MR non-enhanced necrotic lesions, in a total of 10 patients, we diagnosed 6 patients with glioblastoma, found 2 patients had necrotic tissue at >95% and found 2 had

	Age/Gender	MR enhanced active lesion		MR non-enhanced necrotic lesion	Dx	Final Dx
No.		Atypism/Mitosis/Endothelial proliferation/Necrosis	Dx ^a	Atypism/Mitosis/Endothelial proliferation/Necrosis		
1	49/F ^b	+/+/-/-	AA^d	+/+/+/+	GM^{e}	GM
2	72/M ^c	+/+/+/+	GM	+/+/+/+	GM	GM
3	76/M	-/-/+/-	$LGG^{\rm f}$	+/-/+/+	GM	GM
4	58/M	+/+/-/-	AA	-/-/+/+	Only necrosis	GM
5	55/M	+/+/+/+	GM	+/+/-	GM	GM
6	76/F	+/+/-/-	AA	+/-/+/+	GM	GM
7	77/M	+/-/+/+	GM	+/-/+/+	GM	GM
8	59/F	+/+/+/+	GM	-/-/+	Only necrosis	GM
9	58/F	+/+/-	GM	Cystic fluid	Few tumor cells	GM
10	78/F	+/-/+/+	GM	Cystic fluid	Few tumor cells	GM
11	68/M	+/+/+/-	GM	-		GM
12	59/F	+/+/-	GM			GM

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^aDiagnosis; ^bfemale; ^cmale; ^danaplastic astrocytoma; ^eglioblastoma; ^flow grade glioma.

Table II. Statistical analysis: relating factors of T/N ratio.

T/N ratio related factors	No. of patients	P-value	
Cell density			
Grade 1: cystic fluid	2	0.002	
Grade 2: tumor cells with necorsis ≥95%	2		
Grade 3: tumor cells with 50%≤ necrosis <95%	1		
Grade 4: tumor cells with 25%≤ necrosis <50%	3		
Grade 5: tumor cells with necrosis <25%	4		
Grade 6: tumor cells with focal necrosis	10		
LAT1			
Grade 1: <5%	8	0.032	
Grade 2: 5-50%	7		
Grade 3: >50%	2		
MVD ^a		0.057	
EP^{b}		0.24	
Ki-67 LI			
Grade 1: <5%	5	0.741	
Grade 2: 5-25%	6		
Grade 3: 25-50%	2		
Grade 4: >50%	4		

cystic fluid. Four patients with necrotic tissue and cystic fluid did not receive confirmation diagnoses because they did not show enough tumor cells. The diagnostic failure rate was thus 40% (4/10 patients) for biopsy of one non-enhanced lesion. Patient number 4 received a final diagnosis of glioblastoma, reflecting the pathologic features of atypism, endothelial proliferation and necrosis in both lesions.

Pathologic features depending on ¹¹C-methionine uptake and LAT-1 localization. Table II summarizes the pathologic features depending on ¹¹C-methionine uptake. The cell densities were at grade 1 (cystic fluid) in 2, grade 2 (tumor cells with necrosis \geq 95%) in 2, grade 3 (tumor cells with \leq 50% to necrosis <95%) in 1, grade 4 (tumor cells with \geq 25% to <50% necrosis) in 3, grade 5 (tumor cells with necrosis <25%) in 4 and

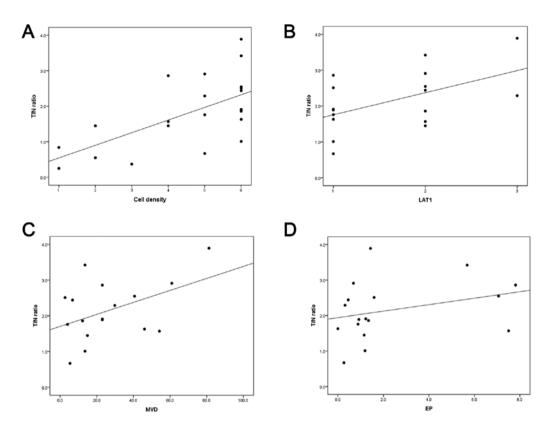


Figure 3. Statistical analysis of correlated factors, depending on the T/N ratio. (A) Cell density correlated statistically with T/N ratio (r=0.629, P=0.002). (B) T/N ratio correlated statistically with LAT1 immunopositivity (r=0.271, P=0.032). (C, D) The MVD (microvessels/mm²) and the number of endothelial proliferations/mm² showed no positive correlations with T/N ratio (r=0.208, P=0.057 and r=0.091, P=0.24, respectively).

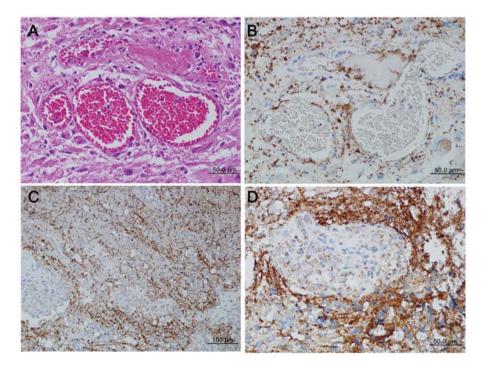


Figure 4. Localization of LAT1. (A) Hematoxylin and eosin staining for glioblastoma. (B) Localization of LAT1 in the endothelium on vessels and cytoplasm in tumor cells. (C, D) Most outside endothelial cells and near tumor cells showed LAT immunopositivity in the areas of endothelial proliferation.

grade 6 (tumor cells with focal necrosis) in 10. We statistically correlated the cell density, depending on the necrotic extent, with the T/N ratio (r=0.629, P=0.002; Fig. 3A). The LAT1

immunopositivity showed a negative expression (grade 1) in 8, a moderate degree of expression (grade 2) in 7 and a high degree of expression (grade 3) in 2. There was a statistical

correlation between the T/N ratio and LAT1 immunopositivity (r=0.271, P=0.032; Fig. 3B). The MVD (microvessels/mm²) and the number of endothelial proliferations/mm² failed to show a positive correlation with T/N ratio (r=0.208, P=0.057 and r=0.091, P=0.24, respectively; Fig. 3C and D). A Ki-67 labeling index appeared in 5 at level <5% (grade 1), 6 at >5% to <25% (grade 2), 2 at >25% to <50% (grade 3) and 4 at level of \geq 50% (grade 4), but it showed no statistical correlation with T/N ratio (r=0.007, P=0.741).

On the immunohistochemical staining, the LAT1 localized in the endothelium in vessels and the cytoplasm in tumor cells. In the areas with endothelial proliferation, most outside endothelial cells and near tumor cells showed immunopositivity (Fig. 4).

Discussion

MRI-guided stereotactic biopsies are performed to identify the nature of an intracranial tumor. Because gliomas are histologically heterogeneous, pathological examinations of stereotactic samples do not always yield their actual grade and extent. Greene et al reported that, in gliomas, the diagnostic yield of CT-guided stereotactic biopsy was 56, 67 and 36% for biopsies performed in the center of the lesion, the enhancing margin, and the hypodense periphery, respectively (14). Furthermore, serial biopsies are needed to minimize the diagnostic failure risk, which reportedly ranges from 1.8 to 7.2% (15,16). To get the essential pathologic features of glioblastomas, such as their endothelial proliferation and/or necrosis, we chose enhanced and non-enhanced lesions corresponding to active and necrotic lesions, respectively. The degree of ¹¹C-methionine uptake was expressed as a ratio to control brain tissue (T/N ratio) and also analyzed along with the various pathologic findings.

First, we analyzed the data comparing MR enhanced lesions and non-enhanced lesions. When we considered the enhanced lesions, we achieved a 66.6% (8 patients out of 12) diagnostic rate, even when all lesions were glioblastomas. Three patients diagnosed with anaplastic astrocytoma each showed two components out of the elements atypism, mitosis, endothelial proliferation and necrosis. One patient showed the features of a low-grade glioma, which was perhaps a marginal tumor area. In biopsies of the non-enhanced areas, we had 60% (6 patients out of 10) glioblastoma diagnostic rates. Two patients had more than 95% necrotic tissue, which meant we could not confirm their diagnoses. Two patients had yellowish cystic fluid containing a few tumor cells, which we could not analyze. When we examined both types of lesions, we got a final diagnosis of glioblastoma in all the cases. One patient had anaplastic astrocytoma in the enhanced portion and necrosis only in the non-enhanced portion. If we combined these features, we could achieve the correct final diagnosis. Therefore, we suggest that biopsies for different targets are needed to minimize the risk of diagnostic failure, and that, in glioblastoma, clinicians can achieve a final diagnosis using biopsies of active and necrotic lesions, even when the lesion's regional heterogeneity provides a serious challenge.

The ¹¹C-methionine PET imaging technique provides functional data that are independent of CT or MRI anatomical images and, in brain tumor cases, giving important information on both histological malignancy and tumor viability (10).

¹¹C-methionine crosses the intact BBB and the tumor cells incorporate it via the neutral amino acid transport system (17,18). Reportedly, this system, the large neutral amino acid transporter 1 (LAT1) is expressed strongly in several tumor cell lines and in tumor endothelial membrane, and it shows a significant correlation with ¹¹C-methionine uptake in human gliomas (6,19-21). Several studies suggest that the degree of ¹¹C-methionine uptake correlates with tumor cell density, proliferative potential, and microvessel density and area in gliomas (8-11). We evaluated each correlated factor according to the ¹¹C-methionine uptake. The T/N ratio showed a statistical correlation with cell density depending on the degree of necrosis and the LAT1 (P=0.002). To show the ¹¹C-methionine uptake localization, we performed immunohistochemical staining on the LAT1. Immunopositivity correlated statistically with T/N ratio (P=0.032) and LAT1 appeared localized in the endothelium of vessels and in the cytoplasm of tumor cells. One study has depicted the localized LAT1 pattern (21). LAT1 expression appeared in the tumor vascular endothelium and tumor cytoplasm and, regarding endothelial proliferations, all layers of vessels showed this immunopositivity (16). Our study showed a similar pattern of expression. However, in endothelial proliferation, most outside endothelial cells and tumor cells near these areas showed a strong positivity for LAT1.

We suggest that multiple stereotactic biopsies of active tumor and necrosis could provide the diagnostic yield in glioblastoma. The ¹¹C-methionine uptake mostly reflected cell densities depending on the degree of necrosis.

Acknowledgements

This study was supported by a grant (CRI11047-1) from the Chonnam National University Hospital Research Institute of Clinical Medicine.

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